

## INTRODUCTION

Fat is a metabolically active component of the human body. Excessive fat in the liver can progress into fibrosis and liver cancer. Chemical-shift encoded magnetic resonance imaging (MRI) [1, 2, 3] has been proven capable of non-invasively quantifying fat fraction in the liver. To work well, these methods require lengthy breath holding and high signal-to-noise (SNR) images. This study aims to develop a free-breathing liver fat and  $R_2^*$  quantification technique using multi-echo radial FLASH and model-based reconstruction (MERLOT).

## METHODS

### Multi-Echo Radial FLASH Sampling

Figure 1 illustrates the implemented multi-echo radial FLASH MRI sequence [4]. After a radio frequency (RF) excitation with the slice-selection gradient ( $G_z$ ), seven echoes with different  $k$ -space spokes are acquired. The acquired echoes are color coded, while the black solid lines indicate either the ramp or the blip gradients.

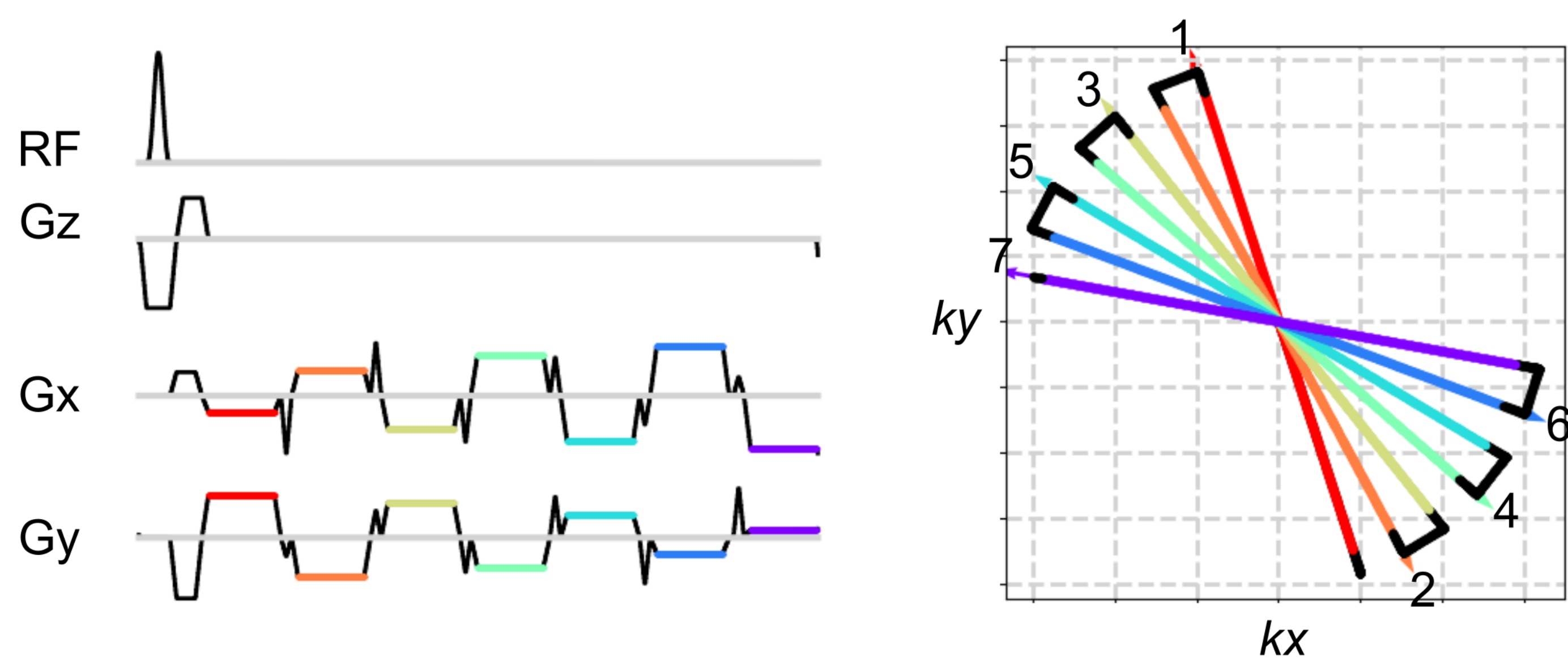


Figure 1: (Left) A repetition block of the multi-echo radial FLASH sequence. (Right) The corresponding  $k$ -space trajectory.

### Model-based Reconstruction

The acquired MR signal,  $y_{j,m}(t)$ , is based on the Fourier transformation:

$$y_{j,m}(t) = \int d\vec{r} e^{-i2\pi\vec{k}(t)\cdot\vec{r}} c_j(\vec{r}) \rho_m(\vec{r}). \quad (1)$$

The sampling trajectory  $\vec{k}(t)$  is from the time integral of readout gradients  $G_x$  and  $G_y$  (see Figure 1). When one image voxel contains both water (W) and fat (F) species, the echo image  $\rho_m$  is modeled as:

$$\mathcal{B} : (W, F, R_2^*, f_{B_0})^T \mapsto \rho_m : (W + F \cdot z_m) \cdot e^{-R_2^* TE_m} \cdot e^{i2\pi f_{B_0} TE_m}. \quad (2)$$

Here,  $z_m = \sum_{p=1}^6 \alpha_p \cdot e^{i2\pi f_p TE_m}$  denotes the six-peak fat spectrum.  $R_2^*$  and  $f_{B_0}$  is the transversal relaxation rate and magnetic field inhomogeneity, respectively. Equations (1) and (2) can be chained together and written in the operator form,

$$y_{j,m} = F_{j,m}(x) := P_m \mathcal{F} M S \mathcal{B}, \quad (3)$$

with  $x = (W, F, R_2^*, f_{B_0}, c_1, \dots, c_N)^T$ .  $F_{j,m}(x)$  denotes the forward operator.  $j$  is the coil index ( $j \in [1, N]$ ), and  $m$  the echo index ( $m \in [1, E]$ ). The nonlinear operator ( $\mathcal{B}$ ) calculates echo images. Every echo image is then point-wise multiplied by a set of coil sensitivity maps in  $x$ , as denoted by  $\mathcal{S}$ . All coil images are then masked to a given field of view ( $M$ ), Fourier-transformed ( $\mathcal{F}$ ), and sampled ( $P$ ) at each echo.

Fat and  $R_2^*$  mapping is achieved via joint estimation of the unknown  $x$ , i.e. minimizing the least square difference between the measured data  $y$  and the forward model under regularizations based on *a priori* knowledge of unknowns,

$$\begin{aligned} & \text{minimize } \|y - F(x)\|_2^2 + \lambda_1 \|\mathcal{W}(E_1 x)\|_1 + \lambda_2 \|\text{TV}_t(E_2 x)\|_1 + \lambda_3 \|x\|_2^2 \\ & \text{subject to } R_2^* \geq 0 \end{aligned} \quad (4)$$

We applied Wavelet regularization and temporal total variation (TV) regularization on the physical parameters in Equation (2),  $\ell^2$  regularization on  $x$ , and non-negativity constraint on  $R_2^*$ .

## EXPERIMENTS

7 subjects (age  $28 \pm 7$ , 1 male) with body mass index  $21.4 \pm 2 \text{ kg m}^{-2}$  participated in this study with written informed consent before MRI in compliance with the regulations established by the local ethics committee. Detailed parameters are flip angle  $5^\circ$ , voxel size  $1.6 \times 1.6 \times 5 \text{ mm}^3$ , echo times (TE) 1.31, 2.54, 3.77, 5.00, 6.23, 7.46, 8.69 ms and repetition time (TR) 9.89 ms. A total scan time of 15 s without breath hold.

## RESULTS & DISCUSSION

Figure 2 shows reconstruction results of two subjects from the proposed MERLOT, and the Siemens reference method, respectively. Clearly, Subject #7 shows elevated FF values in the liver from both methods, indicating fatty liver disease.  $R_2^*$  is a physical quantity linearly proportional to iron concentration.  $R_2^*$  values of both subjects are in the normal range.

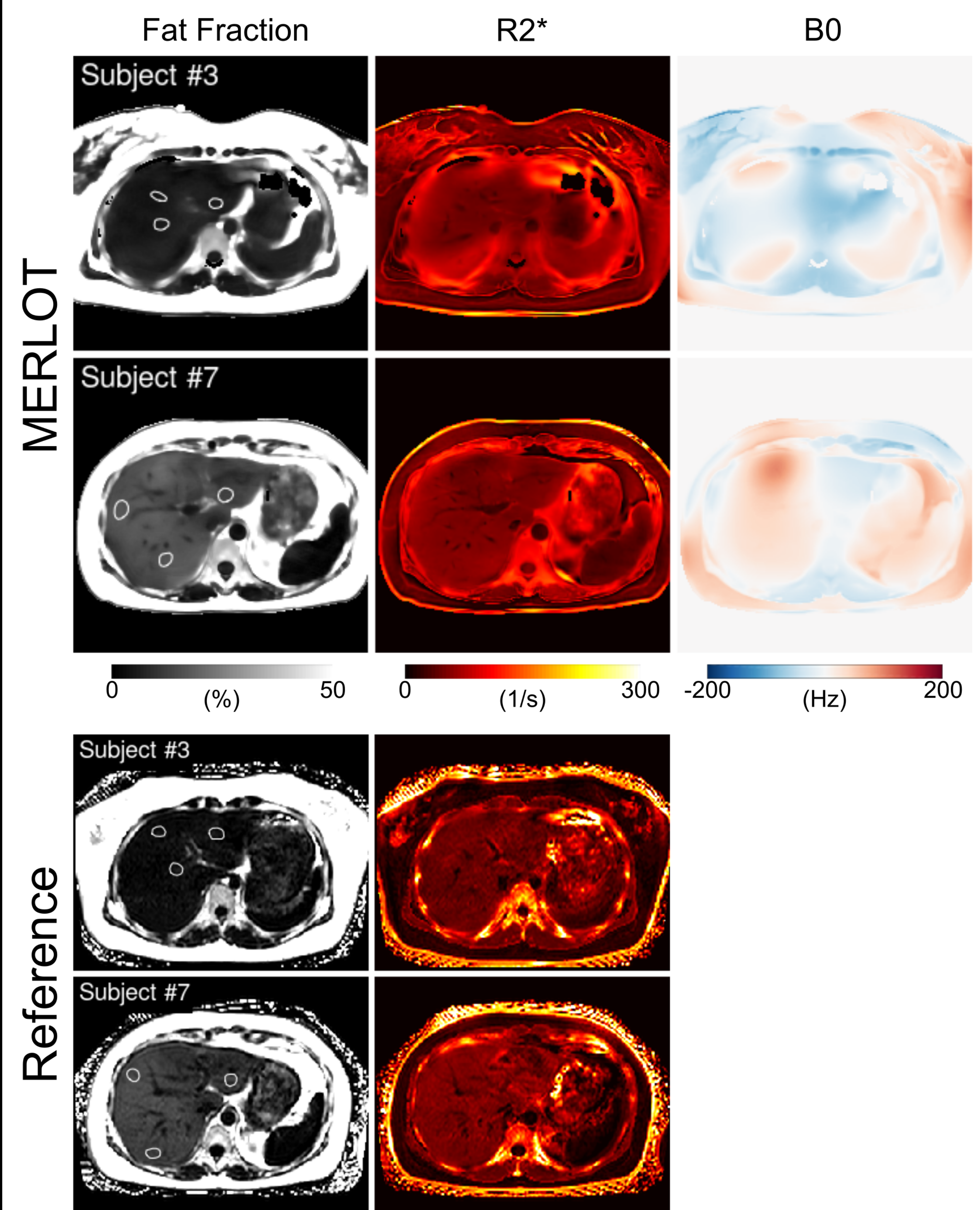


Figure 2: (Top) Fat fraction (FF),  $R_2^*$  and  $B_0$  maps from the proposed MERLOT method. (Bottom) Reference FF and  $R_2^*$  maps from Siemens.

## CONCLUSION

A free-breathing liver fat and  $R_2^*$  mapping technique has been developed and evaluated in subjects with fatty liver disease.

## REFERENCES

- [1] Dixon WT. Simple proton spectroscopic imaging. Radiology (1984).
- [2] Reeder SB, et al. Multicoil Dixon chemical species separation with an iterative least-squares estimation method. MRM (2004).
- [3] Yu H, et al. Multiecho reconstruction for simultaneous water-fat decomposition and  $T_2^*$  estimation. JMRI (2007).
- [4] Tan Z, et al. Dynamic water/fat separation and  $B_0$  inhomogeneity mapping – Joint estimation using undersampled triple-echo multi-spoke radial FLASH. MRM (2019).

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